

# Rapid stepping test towards virtual visual objects: Feasibility and convergent validity in older adults

Yeshayahu Hutzler<sup>a,\*</sup>, Olga Korsensky<sup>a</sup> and Yocheved Laufer<sup>b</sup>

<sup>a</sup>*Academic College at Wingate Institute, Netanya, Israel*

<sup>b</sup>*Department of Physical Therapy, Faculty of Social Welfare and Health Sciences, University of Haifa, Haifa, Israel*

Received 3 July 2016

Accepted 28 July 2016

## Abstract.

**BACKGROUND:** Rapid voluntary stepping has been recognized as an important measure of balance control.

**OBJECTIVE:** The purpose of this study was to assess the feasibility and convergent validity of a Rapid Stepping Test protocol utilizing a virtual reality SeeMe™ system (VR-RST) in elderly ambulatory and independent individuals living in a community residential home.

**METHODS:** Associations between step execution times determined by the system and the Activities-specific Balance Confidence (ABC) Questionnaire, and clinical measures of balance performance in the MiniBESTest and Timed Up and Go (TUG) test, were established in 60 participants (mean age 88.2 + 5.0 years). All participants completed the study.

**RESULTS:** The correlations of the ABC questionnaire and the clinical tests with VR-RST forward and backward stepping were moderate ( $\rho$  range 0.42–0.52), and weak to moderate with sideward stepping ( $\rho$  range 0.32–0.52). Moderate to strong correlations were found across stepping directions ( $\rho$  range 0.45–0.87).

**CONCLUSION:** Findings support the test's feasibility and validity and confirm the utility of the VR-RST as an assessment tool in an elderly population.

Keywords: Balance, assessment, aging

## 1. Introduction

Non-fatal injuries, such as lacerations, hip fractures, and head traumas, which can negatively affect the quality of life and increase the risk of early mortality, are a major health concern due to the growing incidence of falling in the elderly population [1–3]. In addition to the personal threat to these individuals, falls also make up a considerable amount of the elderly's medical expenses [4]. In the U.S., for example, expenses medical expenses due to falls reached about 20 billion dollars in the year 2000 [5], and grew to well over 30 billion dollars in 2013 [6]. According to the U.S. Census Bureau [7], individuals older

\*Corresponding author: Yeshayahu Hutzler, Graduate School, Academic College at Wingate, Wingate Institute, Netanya 42902, Israel. E-mail: shayke@wincol.ac.il.

31 than 85 are considered a unique group and are termed “oldest old” adults, comprising nearly 14% of the  
32 total population older than 65.

33 Impaired balance is commonly considered a primary cause for falling in the elderly, and the risk of  
34 falling increases with age [6,8]. Balance control involves a complex neuromuscular process, demanding  
35 somatosensory, vestibular, and visual input in reference to the environment, in order to keep the body  
36 upright and the line of gravity within the boundaries of the base of support [9–12]. Balance control is  
37 characterized by dynamic, adaptive processes, including (a) proactive (self-initiated and automatically  
38 processed) control, mostly in reference to visual stimuli utilized for surveying the environment for poten-  
39 tial barriers and for preparing a stabilizing strategy in advance, and (b) reactive balance control, which is  
40 characterized by actions in response to unexpected external perturbations, which are generally perceived  
41 through somatosensory stimuli [13]. Each control system contributes to balance control according to the  
42 demands and to the availability of the information. In addition, when one system is deficient the other  
43 system may compensate [11].

44 There are several strategies for responding to balance perturbations; the most commonly used are  
45 ankle and hip strategies [12]. When the ankle and hip strategies are insufficient to prevent a fall that  
46 occurs particularly when perturbations are unexpected and of large amplitude, rapid stepping resulting  
47 in “change in support” is necessary [14]. This is the most effective way to prevent falling [15], but rapid  
48 step execution is often impaired in the elderly [16–18]. Therefore a rapid step execution test (RST)  
49 utilizing a somatosensory cue and force plate measures has been utilized to identify rapid step response  
50 time of elderly individuals at risk for falls. These measures were able to differentiate between fallers  
51 and non-fallers, while the use of functional tests such as the Berg Balance Scale (BBS) and the Timed  
52 Up and Go test (TUG) are less conclusive [19]. In follow-up studies, the RST measure was found to be  
53 valid [20] and reliable [21]. However, force platform assessments are often not feasible in the clinical  
54 setting, due to cost and technological issues. Therefore, efforts have been made to enable the utilization  
55 of RST execution within a more simple, user-friendly, and inexpensive test environment. One solution  
56 for low-cost devices is stepping plates on the floor attached to a video screen [22,23].

57 Virtual reality (VR) systems have acquired an exponentially growing interest in rehabilitation, with  
58 almost two-thirds of the scholarly contributions published about VR systems in rehabilitation directed  
59 toward stroke survivors and the elderly as the main end-users [24–26]). The effectiveness of utilizing  
60 VR technology as an intervention for facilitating mobility and balance after stroke has been established  
61 in a meta-analysis of 16 randomized studies, with a marked effect size after VR training in participants  
62 compared to controls being reported [27]. In addition, the usefulness of this technology for measuring  
63 fall risk in older people has recently been signaled with a specifically designed stepping choice reac-  
64 tion time test [28]. SeeMe<sup>®</sup> Brontes Processing (Gliwice, Poland), an off-the-shelf VR evaluation and  
65 training system that can be tailored by the operating clinician to the capabilities of individuals with im-  
66 pairments [22–24], was developed by a physiotherapist team during the first decade of the 21st century  
67 and reliably applied for upper extremity reaching [29]. However, until now, no RST has been described  
68 utilizing on an off-the-shelf VR platform using only a computer, a video camera, and a screen. Follow-  
69 ing preliminary results with the SeeMe VR system, previously presented in a conference poster [30], the  
70 objectives of the present study were to assess RST in the forward, sideward, and backward directions,  
71 and to inform the convergent validity of these tests by means of associations between step execution time  
72 as determined by the SeeMe system and clinical measures of balance performance and fear of falling. A  
73 secondary purpose was to assess the impact of age across measures.

---

	All	≥ 86	≤ 85
<i>N</i> of participants (males/females)	60	42 (8/34)	18 (4/14)
Age (Mean ± SD)	88.2 ± 5	90.7 ± 3.5	82.3 ± 2.3
<i>N</i> falling in past year	18	14	4
<i>N</i> using assistive devices at home	10	9	1
<i>N</i> using assistive devices outside the home	21	19	2
<i>N</i> (Mean ± SD) of exits from residence	4.2 ± 5.2	6.2 ± 5.4	1.2 ± 4.8
<i>N</i> (Mean ± SD) of weekly physical activity sessions	7.1 ± 1.9	8.1 ± 1.8	1.76 ± 2

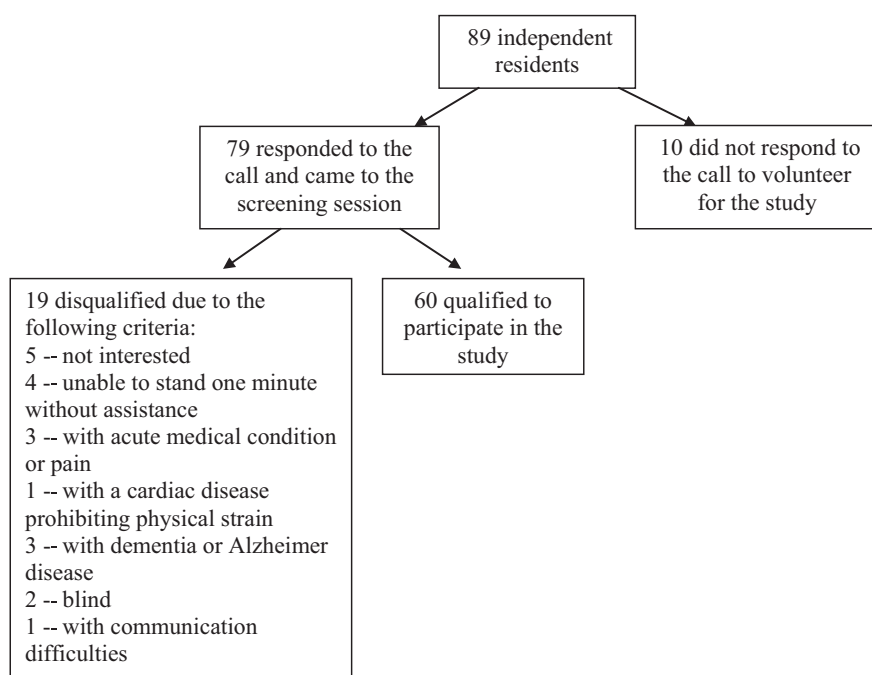


Fig. 1. Selection of participants to the study.

## 2. Methods

### 2.1. Participants

All independent residents of a senior living retirement center targeting a middle-class Caucasian population were invited to participate in this study. Sixty volunteers (mean age  $88.2 \pm 5.0$  years) residing in this center participated in the study. The inclusion criteria were: (a) age above 65; (b) able to walk independently with/without assistive devices; (c) able to respond to auditory and visual instructions and stimuli; and (d) willing to sign the consent form. The exclusion criteria were: (a) medical conditions prohibiting the ability to perform the MiniBEST balance test [31,32]; and (b) having an acute injury, a disease, or acute pain. Figure 1 describes the participants' selection process. Our sample included a large cohort of "oldest old" adults, and in order to reflect the specific sensitivity of our system for balance control with growing age, the RST and clinical balance outcomes within our sample were compared across age subgroups. The participants were divided into two subgroups of participants: aged 85 and below

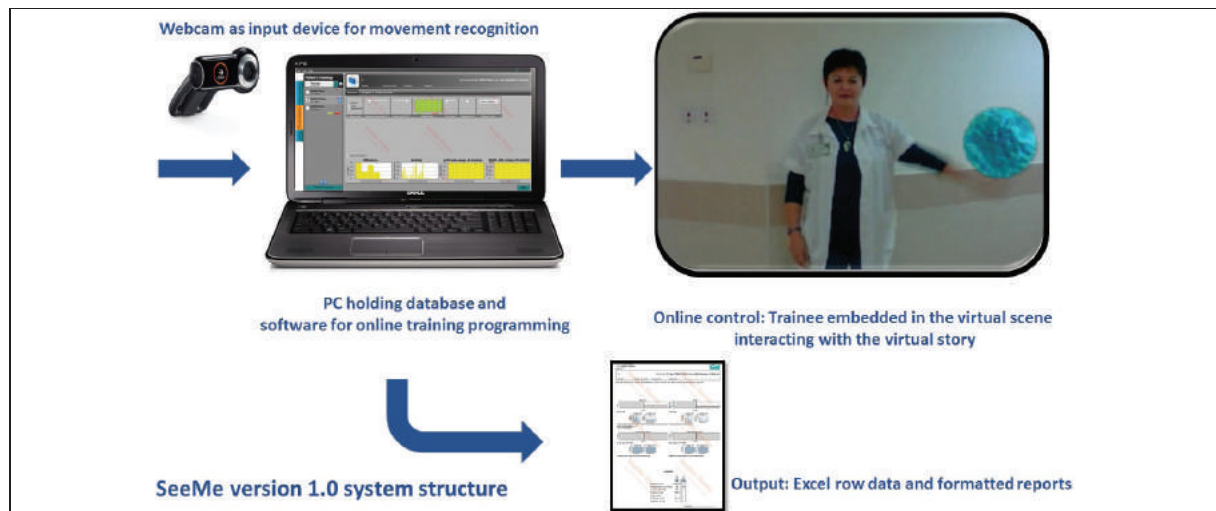


Fig. 2. SeeMe system structure.

86 ( $n = 18$ : 4M; 14F), and aged 86 and above (“oldest old”;  $n = 42$ : 8M; 34F). Table 1 describes the  
 87 participants’ background variables related to their functional and community participation details rele-  
 88 vant to balance and mobility. The study was approved by the Institutional Ethical Review Board of the  
 89 Faculty. An informed consent form was signed by all the individuals participating in the study.

## 90 2.2. Instruments

### 91 2.2.1. SeeMe platform

92 SeeMe<sup>®</sup> Version 1.0 (Brontes Processing, Gliwice Poland) is a clinician-controlled exercise and as-  
 93 sessment system utilizing projected video capture by means of a webcam and Microsoft Kinect technol-  
 94 ogy, a PC, and a 42-inch LCD screen. The design and structure of the SeeMe system are demonstrated  
 95 in Fig. 2. The off-the-shelf system consists of several games.

### 96 2.2.2. VR react game

97 In this game, virtual balls appear randomly at predetermined distances on both sides of the screen (see  
 98 Fig. 3). In this task the participant touches the virtual ball with his/her arm or foot. The system records  
 99 the response time and the number of correct actions vs. misses. In the current study a specific setup and  
 100 protocol of this game was used, labeled the *Virtual Reality Rapid Stepping Test (VR-RST)*. This protocol  
 101 included one 90 sec training session, and three 60 sec-long testing sessions of the React game within the  
 102 SeeMe VR platform.

103 The game was projected on a 42-inch TV screen. A webcam was located 50 cm above the floor,  
 104 150 cm away from the participant, who stood within a 30 cm square area marked with tape on the floor.  
 105 The camera was rotated at an angle of 30 degrees toward the highlighted square. Four sets of trials were  
 106 programmed and executed, the first (a) for habituation and the others (b–d) for measurement:

107 (a) A 90 sec acclimatization game, in which each participant gained some experience with the game  
 108 environment. The participant interacted with the game for 30 sec while facing the camera and  
 109 executing side stepping. This was followed by two periods of 30 sec facing the screen with either  
 110 the left or right side of the body, and executing forward and backward steps with the right and left  
 111 foot, as appropriate;

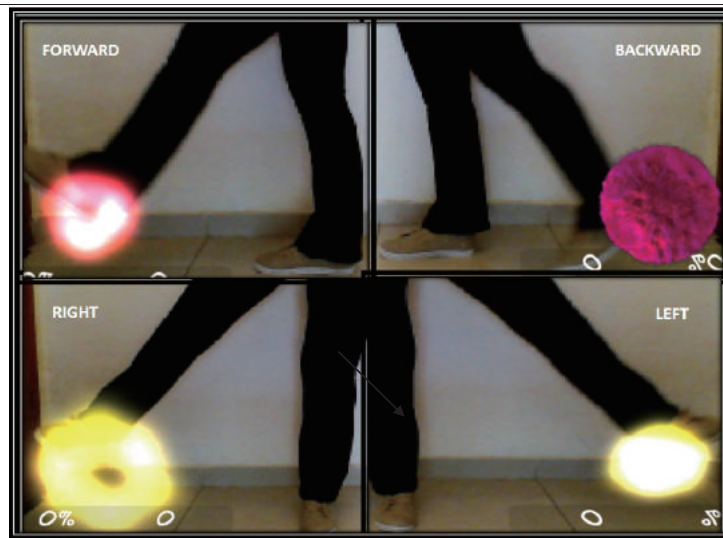


Fig. 3. Step test in the SeeMe system.

112 (b) A 60 sec series of game interactions at the frontal plane;

113 (c) A 60 sec series of game interactions with the right side to the camera and screen, in which the  
114 right foot executed the steps forward or backward; and

115 (d) A 60 sec series of game interactions with the left side to the camera and screen, in which the left  
116 foot executed the steps forward or backward.

117 During each of the three actual test series (frontal, right foot, left foot), the system was set to project  
118 on the screen 10 balls per 30 sec, for a total of 20 balls for the 60 sec game. The participant started each  
119 game while standing on a square area marked by tape. The instructions were to step toward the target  
120 as soon as it appeared, as fast as possible. The balls appeared at random on the participant's left or right  
121 and frontal or backward direction. If the participant did not manage to touch a ball within a given time of  
122 3 sec, the ball disappeared and another ball appeared at a random spot on the screen (50% to the left or  
123 right in the frontal plane and forward or backward in the sagittal plane games). The median step response  
124 time was calculated out of all the steps performed in each direction (right, left, forward, backward).

### 125 2.2.3. *Activities-specific Balance Confidence (ABC) scale*

126 This is a 16-item self-report questionnaire that asks individuals to rate their balance confidence in per-  
127 forming specific ambulatory activities, on a numerical rating scale of 0–100. A score of zero represents  
128 no confidence, while a score of 100 represents complete confidence in performing the activity. The scale  
129 was found reliable in elderly and post-stroke populations [33,34], and is often used as an indication of  
130 fear of falling [35].

### 131 2.2.4. *MiniBESTest*

132 The original Balance Evaluation Systems Test (BESTest) was developed as a clinical balance as-  
133 sessment tool that aims at targeting different balance control systems, so that specific rehabilitation  
134 approaches can be designed for different balance deficits [36]. This 36-item version was later abridged  
135 into a more practical system called the Mini-BESTest [32]. This test is comprised of 14 items, retaining  
136 four out of the six balance categories (anticipatory postural adjustments, postural responses, sensory

	All	$\geq 86$	$\leq 85$
Forward step:	1133	1178.75	1054
Median (range)	(866–2300)	(866–2091.5)	(916–2300)
Backward step:	1083	1083	1049.5
Median (range)	(824.5–2433)	(833–2433)	(824.5–2200)
Sideward step:	1037	1045.5	1028.5
Median (range)	(866–2116)	(866–2116)	(891.5–1750)

	All	$\geq 86$	$\leq 85$
TUG (sec)	12.2 $\pm$ 6.2	12.7 $\pm$ 7	11 $\pm$ 3.4
MiniBESTest score	20.3 $\pm$ 5.3	19.3 $\pm$ 5.2	22.6 $\pm$ 4.7
MiniBESTest (%)	72.5 $\pm$ 18.8	69 $\pm$ 18.7*	80.75 $\pm$ 16.8
ABC (%) Mean $\pm$ SD	80.4 $\pm$ 3.7	80.8 $\pm$ 14	80.2 $\pm$ 13.7

Note: \* = Between group t-test significant at  $p < 0.05$ .

orientation, and balance during gait) from the original BESTest, and can be conducted within a time of 15 minutes [37].

### 2.2.5. Timed Up and Go (TUG)

This is a quick, simple, and widely-used clinical outcome measure of lower extremity function, fall risk, and mobility [38]. In this test participants are asked to stand up from sitting in a standard-height chair, walk a distance of 3 m (marked on the floor) at a comfortable pace, turn, walk back, and sit down again. Participants are allowed to use routine walking aids and are instructed not to use their arms to stand up. The TUG is a part of the MiniBESTest, but is often used as a stand alone test to assess functional mobility. Scoring in the MiniBESTest is on an ordinal scale, while in the TUG the number of seconds needed to complete the test is recorded with a stopwatch. Timing starts on the command "Go" and stops when the participant's back is positioned against the back of the chair after sitting down again [39,40].

### 2.3. Procedure

After reading and signing the informed consent form, the participants completed a demographic questionnaire and the ABC questionnaire. They then performed the functional balance assessment utilizing the MiniBESTest (14 sub-test), including the TUG. After a 2-min rest period they completed the VR-RST. The entire procedure lasted about one hour.

### 2.4. Statistical analysis

Since the outcomes of VR-RST did not present a normal distribution, non-parametric statistics were used. RST times are presented in median and range. Spearman Rank correlations were computed to describe the correlation between the VR-RST and the functional balance measurements (Mini-BEST and TUG) or and between the VR-RST and the fear of falling scale (ABC). Significance was set at  $p \leq 0.05$ . Benchmarks for correlations were  $r \leq 0.35$  considered as low or weak correlations,  $r$  between 0.36 to 0.67 modest or moderate correlations, and  $r$  between 0.68 to 0.90 as strong or high correlations.

Age/measure	Forward step			Backward step			Sideward step		
	All	≥ 86	≤ 85	All	≥ 86	≤ 85	All	≥ 86	≤ 85
Forward step				0.60***	0.62***	0.58*	0.57***	0.59***	0.45*
Backward step	0.85***	0.87***	0.76***				0.57***	0.59***	0.45
Sideward step	0.60***	0.62***	0.58*	0.57***	0.59***	0.45			

Note: \* =  $p < 0.05$ ; \*\* $p < 0.01$ ; \*\*\* $p < 0.001$ .

Age/measure	Forward step			Backward step			Sideward step		
	All	≥ 86	≤ 85	All	≥ 86	≤ 85	All	≥ 86	≤ 85
TUG	0.46***	0.39***	0.59***	0.42***	0.32	0.72***	0.37**	0.45**	0.15
MiniBESTest	-0.52***	-0.46***	-0.59**	-0.52***	-0.45**	-0.61**	-0.32**	-0.41**	-0.17
ABC	-0.35**	-0.35*	-0.28	-0.46***	-0.43**	-0.6**	-0.35**	-0.43**	-0.09

Note: \* =  $p < 0.05$ ; \*\* $p < 0.01$ ; \*\*\* $p < 0.001$ .

with  $r$  coefficients  $\geq 0.90$  as very high correlations [41]. While not the primary purpose of the study, age groups were compared via t-tests to assess the hypothesis that the “oldest old” would have lower outcomes compared to those of the less old.

### 3. Results

All participants completed the study. The median and range of the VR-RST scores are presented in Table 2. The means and SD scores of the clinical functional tests (Mini-BESTest and TUG) and the ABC questionnaire are presented in Table 3. The correlations between the VR-RST sub-domains, i.e., stepping forward, backward, and sideward, are all strong, and are presented in Table 4, while the correlations between the VR-RST and the clinical tests are presented in Table 5. Significant moderate to strong correlations were determined between the VR-RST in all directions and weak to moderate correlations were determined between the VR-RST and the Mini-BESTest, the TUG test, and the ABC questionnaire. The correlations between the Mini-BESTest and the forward and backward steps ( $\rho = -0.52$ ) were higher than the correlation between the Mini-BESTest and the sideward steps ( $\rho = -0.32$ ). Similarly, the correlations between the TUG test and the forward and backward steps ( $\rho = -0.46$  and  $-0.42$ , respectively) are higher than between the TUG test and the sideward test ( $\rho = -0.37$ ). A different pattern emerged regarding the correlations between the ABC and steps in different directions, as the strongest correlation was with backward steps ( $\rho = -0.46$ ), whereas the correlation with the forward and sideward steps were both  $\rho = -0.35$ .

When comparing the groups of old (85 years and below) and very old adults (above 85 years), we did not find any significant differences in the TUG functional test, ABC questionnaire, or VR-RST results. However, we did find significant differences across age groups in the MiniBESTest ( $t_{1,58} = -2.4$ ;  $p < 0.03$ ).

### 4. Discussion

In spite of the age of the participants (nearly two-thirds were above 85 years old), no adverse effects occurred while executing the tests. The durations of the rapid steps performed within the VR-RST setup

186 with the SeeMe platform, with median scores of 1133, 1083, and 1037 ms for forward, backward, and  
187 sideward stepping, respectively (see Table 2), are in agreement with RST to somatosensory cues by  
188 means of force plate measurement [19]. The VR-RST scores appear to be very similar to the outcomes  
189 of the choice reaction test in the frontal plane performed by 104 elderly individuals in an Australian  
190 study, which revealed mean total step times equal to  $1231 \pm 242$  ms for fallers and  $1113 \pm 151$  for  
191 non-fallers [28]. The values of the non-fallers in the latter study are within the range of the findings in  
192 our sample, in which two-thirds were comprised of non-fallers.

193 Step durations in the current study seem to be moderately to strongly associated with commonly-used  
194 clinical measures of balance performance in the elderly. The strongest association was with the Mini-  
195 BESTest, which provides a comprehensive measure of balance in the elderly. The Spearman correlations  
196 found in our study of the RST with the TUG test and the ABC questionnaire were stronger than those  
197 found in a study of 167 elderly adults with a 10-year younger mean age than in our sample, which  
198 used a different version of the RST, averaging  $\rho = 0.346$  and  $0.321$ , respectively [42]. However, in  
199 the latter version of the RST, a different outcome measure was used, i.e., the total time of 24 steps  
200 in forward, backward, and sideward directions, and the response was performed to the experimenters'  
201 verbal commands rather than to visual cues.

202 Several sources of information indicate that elderly persons are more likely to experience posterior  
203 rather than anterior or lateral falls. For example, in a study of 242 older adults (mean age  $80 \pm 4.4$  years),  
204 it was found that reactions to perturbations in the posterior direction best discriminated between those  
205 who reported falling in the past 12 months and those who did not [43]. In an earlier study that examined  
206 protective mechanisms while falling, it was determined that pelvic impact was involved in more than  
207 90% of the posterior falls, but in only 23% of the lateral falls and in none of the anterior falls [44]. Based  
208 on these findings, it may be expected that the elderly will develop a more prominent fear of falling back-  
209 ward rather than towards other directions, as is reflected in our finding of stronger negative association  
210 between the backward steps in the VR-RST and the total ABC score (Table 5). Those who have a faster  
211 backward step response appear to be more confident in keeping their balance while backward stepping.

212 The TUG involves mostly locomotor activity in the posterior-anterior plane. Similarly, the Mini-  
213 BESTest's score is composed of 14 tasks that represent a variety of activities, with only two of them in  
214 the lateral plane [34]. The stronger association of these tests with response time in forward and backward  
215 step execution using the VR-RST is another indication for the validity of the proposed VR assessment  
216 method.

217 The lack of differences in the VR-RST between the old and "oldest old" groups in most variables as  
218 revealed in our study is noteworthy, since research typically indicates a deterioration in balance capabili-  
219 ties with aging [45,46]. One reason for the lack of such a finding in our sample might be the participants'  
220 relatively high degree of functioning, with only one-third having experienced falls in the previous year.

## 221 5. Conclusions

222 The VR-RST system described in this study appears to be a safe and valid measurement device in  
223 elderly ambulatory and independent individuals living in a community residential home. The fast-step  
224 duration times measured by means of the VR-RST system in this sample of older adults exhibited mod-  
225 erate significant correlations with functional balance tests, and were within the range of force plate  
226 measurements in other studies for a similar task. Therefore, based on these results, we suggest that the  
227 VR-RST may be a useful tool for clinicians working with a geriatric population, or any other population  
228 experiencing balance disorders. Future studies are warranted to evaluate the repeatability of results in

---



229 the same participants, as well as the sensitivity and specificity for fall detection. Other studies evaluating  
230 the responsiveness of the VR-RST are also needed, and their results should, again, be compared to the  
231 findings of clinical tests. If satisfactory outcomes are revealed, the VR-RST may be further implemented  
232 as a tele-measurement system for balance assessment, which may save administration costs as well as  
233 increase the individual's independence regarding his or her assessment and training process.

### 234 **Conflict of interest**

235 The authors declare no conflict of interest regarding the publication of this study. The first and third  
236 authors are academic researchers, and the second author was at the time of study a graduate student  
237 performing her thesis research.

### 238 **References**

- 239 [1] Centers for Disease Control and Prevention (CDC), National Center for Injury Prevention and Control. Web – based  
240 Injury Statistics Query and Reporting System (WISQARS). Older adult falls. [http://www.cdc.gov/HomeandRecreation-  
242 alSafety/Falls/adultfalls.html](http://www.cdc.gov/HomeandRecreation-<br/>241 alSafety/Falls/adultfalls.html).
- 243 [2] Sterling DA, O'Connor JA, Bonadies J. Geriatric falls: Injury severity is high and disproportionate to mechanism. *Journal  
244 of Trauma – Injury, Infection and Critical Care*. 2001; 50(1): 16-119.
- 245 [3] Alexander BH, Rivara FP, Wolf ME. The cost and frequency of hospitalization for fall – related injuries in older adults.  
246 *American Journal of Public Health*. 1992; 82(7): 1020-1023.
- 247 [4] Rao SS. Prevention of falls in older patients. *American Family Physician*. 2005; 72(1): 81-88.
- 248 [5] Stevens JA, Corso PS, Finkelstein EA, Miller TR. The costs of fatal and non-fatal falls among older adults. *Injury  
249 Prevention*. 2006; 12(5): 290-295.
- 250 [6] Centers for Disease Control and Prevention CDC, Older Adult Falls: Get the Facts Online: [http://www.cdc.gov/home-  
252 andrecreationalsafety/falls/adultfalls.html](http://www.cdc.gov/home-<br/>251 andrecreationalsafety/falls/adultfalls.html).
- 253 [7] U.S. Census Bureau, 2011, Age and sex composition: 2010, by LM Howden and JA Meyer, 2010 Census Briefs,  
254 C2010BR-03, available at <http://www.census.gov/prod/cen2010/briefs/c2010br-03.pdf>.
- 255 [8] Tinetti ME, Kumar C. The patient who falls. *Journal of the American Medical Association*. 2010; 303(3): 258-266.
- 256 [9] Horak FB. Postural orientation and equilibrium: what do we need to know about neural control of balance to prevent  
257 falls? *Age Ageing*. 2006; 35(2): ii7-ii11.
- 258 [10] Zajonc TP, Roland PS. Vertigo and motion sickness. Part I: vestibular anatomy and physiology. *Ear, Nose & Throat  
259 Journal*. 2005; 84: 581-584.
- 260 [11] Herdman S. Vestibular rehabilitation, 3rd edn. F.A. Davis, Philadelphia, PA, 2007.
- 261 [12] Shumway-Cook A, Woollacott MH. Motor control: Translating research into clinical practice, 4th edn. Lippincott,  
262 Philadelphia, PA, 2011.
- 263 [13] Huxham F, Goldie P, Patela A. Theoretical considerations in balance assessment. *Australian Journal of Physiotherapy*.  
264 2001; 47: 89-100.
- 265 [14] Maki BE, McIlroy WE. Control of rapid limb movements for balance recovery: age-related changes and implications for  
266 fall prevention. *Age and Ageing*. 2006; 35(2): ii12-ii18.
- 267 [15] Patla E, Frank JS, Winter DA et al. Age-related changes in balance control system: initiation of stepping. *Clinical  
268 Biomechanics*. 1993; 8: 179-184.
- 269 [16] Maki E, McIlroy WE. Effects of aging on control of stability. In: A textbook of audiological medicine: Clinical aspects of  
270 hearing and balance. Luxon L, Martini A, Furman J, Stephens D, eds, Martin Dunitz Publishers, London, 2003; 671-690.
- 271 [17] Mancini M, Horak FB. The relevance of clinical balance assessment tools to differentiate balance deficits. *European  
272 Journal of Physical and Rehabilitation Medicine*. 2010; 46(2): 239-249.
- 273 [18] Schoene D, Smith ST, Davies TA et al. A Stroop Stepping Test (SST) using low-cost computer game technology dis-  
274 criminates between older fallers and non-fallers. *Age and Ageing*. 2014; 43(2): 285-289. doi: 10.1093/ageing/aft157.
- 275 [19] Melzer I, Kurz D, Shahar M et al. Application of the voluntary step execution test to identify elderly fallers. *Age and  
276 Ageing*. 2007; 36: 532-537.
- 277 [20] Melzer I, Kurz I, Sarid O, Jette AM. Relationship between self-reported function and disability and balance performance  
measures in the elderly. *Journal of Rehabilitation Research & Development*. 2007; 44(5): 685-692.

- 277 [21] Melzer I, Shtilman I, Rosenblatt N, Oddsson LIE. Reliability of voluntary step execution behavior under single and dual  
278 task conditions. *Journal of NeuroEngineering and Rehabilitation*. 2007; 4: 16.
- 279 [22] Lord SR, Fitzpatrick RC. Choice stepping reaction time: A composite measure of falls risk in older people. *The Journals*  
280 *of Gerontology Series A: Biological Sciences and Medical Sciences*. 2001; 56(10): M627-M632.
- 281 [23] Yamaji S, Demura S, Sohee S, Uchiyama M. Reliability of a new rapid step test for older women and its relationship  
282 with fall risk and leg muscle function. *Health*. 2012; 4(1): 703-711. <http://dx.doi.org/10.4236/health.2012.429110>.
- 283 [24] Laufer Y, Sugarman H, Burstin A, Brown R. Age, but not sit or stance, affects rapid reaching movement time to virtual  
284 objects in response to a simple or choice cue. Presented at the Joint World Congress of ISPGR and Gait & Mental  
285 Function, Trondheim. 2012; [http://ispgr.org/fileadmin/templates/\\_img/norway2012/ISPGR\\_Detailed\\_Program\\_2012\\_04\\_26.pdf](http://ispgr.org/fileadmin/templates/_img/norway2012/ISPGR_Detailed_Program_2012_04_26.pdf).
- 286 [25] Hutzler Y. Virtual reality and exergaming in rehabilitation: Scientific evidence and practical impact on adapted physical  
287 activity (APA), *Spor Bilimler Dergisi. Hacettepe Journal of Sport Sciences*. 24(2): 80-84.
- 288 [26] Laufer Y, Dar G, Kodesh E. Does a Wii-based exercise program enhance balance control of independently functioning  
289 older adults? A systematic review. *Clinical Interventions in Aging*. 2014; 9: 1803-1813.
- 290 [27] Li Z, Han XG, Sheng J, Ma SJ. Virtual reality for improving balance in patients after stroke: A systematic review and  
291 meta-analysis. *Clinical Rehabilitation*. 3 Jul 2015. pii: 0269215515593611. [Epub ahead of print].
- 292 [28] Ejupi A, Brodie M, Gschwind YJ et al. Choice stepping reaction time test using exergame technology for fall risk assess-  
293 ment in older people. *Conf Proc IEEE Eng Med Biol Soc*. 2014; 2014: 6957-60. doi: 10.1109/EMBC.2014.6945228.
- 294 [29] Brown R, Burstin A, Laufer Y. Age but not sit or stance affects rapid reaching movement time to virtual objects in  
295 response to a simple or go/no-go task. *PM&R Journal*. 2014; 6(8, 2): S126-S127.
- 296 [30] Laufer Y, Burstein A, Brown R, Korsensky O, Hutzler Y. Rapid stepping time on virtual objects correlates with measures  
297 of balance and fear of falling in elderly individuals. *WCPT Congress, Physiotherapy*. 2015; 101, Supplement 1 eS189.  
298 doi: <http://dx.doi.org/10.1016/j.physio.2015.03.349>.
- 299 [31] O'Hoski S, Sibley KM, Brooks D, Beauchamp MK. Construct validity of the BESTest, mini-BESTest and briefBESTest  
300 in adults aged 50 years and older. *Gait & Posture*. 2015; 42(3): 301-305. DOI: <http://dx.doi.org/10.1016/j.gaitpost.2015.06.006>.
- 301 [32] Franchignoni F, Horak F, Godi M et al. Using psychometric techniques to improve the balance evaluation systems test:  
302 The mini-BESTest. *Journal of Rehabilitation Medicine*. 2010; 42(4): 323-231. doi: 10.2340/16501977-0537.
- 303 [33] Powell LE, Myers AM. The activities-specific balance confidence (ABC) scale. *Journal of Gerontology, Series A: Bio-*  
304 *logical Sciences & Medical Sciences*. 1995; 50(1): 28-34.
- 305 [34] Botner EM, Miller WC, Eng JJ. Measurement properties of the Activities-specific Balance Confidence Scale among  
306 individuals with stroke. *Disability & Rehabilitation*. 2005; 27(4): 156-163.
- 307 [35] Klima DW, Newton RA, Keshner EA, Davey A. Fear of falling and balance ability in older men: the priest study. *Journal*  
308 *of Aging and Physical Activity*. 2012; 21(4): 375-386. Epub 2012 Nov 19.
- 309 [36] Horak R, Wrisley DM, Frank J. The Balance Evaluation Systems Test (BESTest) to differentiate balance deficits. *Physical*  
310 *Therapy*. 89(5): 484-498.
- 311 [37] Godi M, Franchignoni F, Caligari M et al. Comparison of reliability, validity, and responsiveness of the mini-  
312 BESTest and Berg Balance Scale in patients with balance disorders. *Physical Therapy*. 2013; 93(2): 158-67. doi:  
313 10.2522/ptj.20120171.
- 314 [38] Podsiadlo D, Richardson S. The timed 'Up & Go': a test of basic functional mobility for frail elderly persons. *Journal of*  
315 *the American Geriatric Society*. 1991; 39: 142-148. [PubMed].
- 316 [39] Giladi N, Herman T, Reider-Groswasser II et al. Clinical characteristics of elderly patients with a cautious gait of un-  
317 known origin. *Journal of Neurology*. 2005; 252: 300-306.
- 318 [40] Vereeck L, Wuyts F, Truijien S, Van de Heyning P. Clinical assessment of balance: normative data, and gender and age  
319 effects. *International Journal of Audiology*. 2008; 47: 67-75.
- 320 [41] Taylor R. Interpretation of the correlation-coefficient – A basic review. *Journal of Diagnostic Medical Sonography*. 1990;  
321 6: 35-39.
- 322 [42] Cho B, Scarpace D, Alexander NB. Tests of stepping as indicators of mobility, balance, and fall risk in balance-impaired  
323 older adults. *Journal of the American Geriatrics Society*. 2004; 52: 1168-1173.
- 324 [43] Sturnieks DL, Menant J, Delbaere K et al. Force controlled balance perturbations associated with falls in older people: a  
325 prospective cohort study. *PLoS One*. 9 Aug 2013; 8(8): e70981. doi: 10.1371/journal.pone.0070981.
- 326 [44] Hsiao ET, Robinovitch SN. Common protective movements govern unexpected falls from standing height. *Journal of*  
327 *Biomechanics*. 1998; 31(1): 1-9.
- 328 [45] Jiang J, Long J, Ling W et al. Incidence of fall-related injury among old people in mainland China. *Archives of Geron-*  
329 *tology and Geriatrics*. 2015; 61(2): 131-139. doi: 10.1016/j.archger.2015.06.003. Epub 2015 Jun 12.
- 330 [46] Cattagni T, Scaglioni G, Cornu C et al. What are the effects of the aging of the neuromuscular system on postural  
331 stability? *Geriatrics Psychol Neuropsychiatr Vieil*. 1 Dec 2015; 13(4): 363-380.
- 332
- 333
-